Rapid PCR for Integration in Sample-to-answer Analysis Platforms



By employing simulation methods such as CFD,

optimum heat transfer conditions were identified.

Based on these findings a chip layout for fast and

robust PCR was devised that runs 30 PCR cycles in

6 minutes. Most prominently, performance verifica-

tions were provided by testing of real samples con-

taining genomic DNA both, from purified nucleic

acids and not pre-treated whole blood. Employing

simulation methods and analysing experimental

results ended-up in a fast and robust PCR set-up

including appreciation of key processes. Notably, the module has the potential of integration to com-

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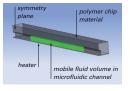
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Introduction

Polymerase chain reaction (PCR) nowadays constitutes an important and commonly applied method for a plenitude of diagnostics such **as medical diagnostics of infectious diseases.** Compared to conventional approaches such as Gram staining and cell/bacteria culturing, molecular tests are often not only **faster** but also **yield rather specific information**, e.g. on the type of pathogenic agents present. Results from molecular tests thereby render specific and **highly efficient therapy feasible**, in particular, when implemented in systems providing results directly at **the point of care** (POC). Here, a rather elegant solution to integrate a fast PCR in POC systems is presented, based on the **moving plug concept**.

System Design and Results

CFD simulation (ANSYS CFX) using a moving mesh as fluid plug inside a mesh representing the polymer chip surrounding the channel.

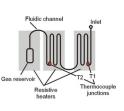


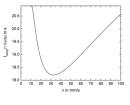
Characteristic **time scales for different transport phenomena.** Diffusion time scales are calculated for half of the channel height: $t = x^2 / (2 D)$ t: time, x= 1/2 channel height, D: diffusion coefficient.

Plug velocity v in mm/s	Internal rotation t in s			Diff. mass transport t in s				Diff. heat transport t in s			
Plug #	1	2	3	1		2	3		1	2	3
10	9.6	6.3	1.7	20) 3	36	111		0.3	0.5	1.9
40	2.4	1.6	0.4	20) 3	36	111		0.3	0.5	1.9
70	14	0.9	0.2	20	1 5	86	111		0.3	0.5	19

Design rationale: The plug is moved back and forward against a closed reservoir ("dead end") by air pressure built up by a syringe pump (similar to systems reported in [2, 3]). Wettability effects such as corner flow are reduced, because the actuating pressure built up by the pump is significantly higher than the Laplace pressures stemming from surface tension effects. The dead end reservoir is heated to avoid condensation and hence loss of reaction volume.

The overall cycling time is comprised of heating/cooling time and travelling time of the moving plug. Fastest cycling times are found as a compromise between times required when the hold position over a heating zone is reached and velocity of the fluid plug. (high velocity means longer heating/cooling time but shorter travelling time).





Minimum in overall cycling time computed from experimental temperature profiles.

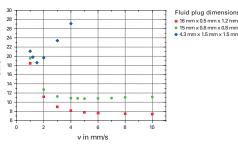
Internal vortices enhance mixing of reagents mass transfer is dominated by convection.

CD-Medics) [1].

Heat transfer dominated by diffusion processes (see Table left for estimates of characteristic time scales). Heater is located below the sealing foil of the channel.



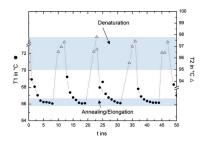
iMM



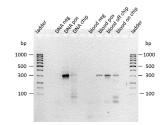
plex sample-to-answer platforms.

From simulations the times t when the final temperature is nearly reached are analysed (here: 98 % of T difference).

Heat transfer rates are determined by a) shape (diameter, length) and b) velocity of fluid plug. A diameter in the range of best performance in terms of rapid heat transfer is chosen. Optimum velocity is determined from experiments.



Typical temperature profile of the fluid plug obtained in experiments.



Results from successful PCRs using **purified genomic DNA, centrifuged blood** (blood off chip), <u>whole blood</u> (blood on-chip). Positive tests were carried out in a conventional cycler using lysed and centrifuged blood.



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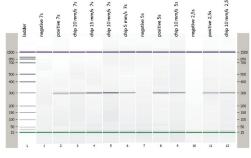




Fluid plug (stained by red food colour) moving from one tempera-

Microfluidic cartridge for HLA typing POC application (EC project

ture zone to the next. (Experiments carried out on a stand-alone PCR device.)



Results obtained during **optimisation of the PCR protocol in terms of cycling time**. best results at plug velocity of 10 mm/s and 7 s annealing/elongation.