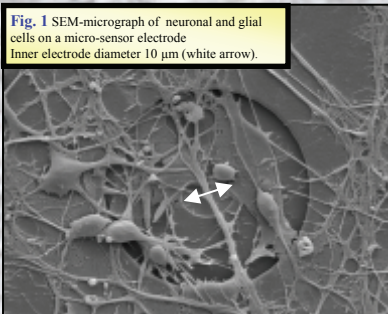




A new exposure system for the *in vitro* detection of GHz field effects on neuronal networks

Introduction

Different ideas exist about possible targets for biological effects of electromagnetic fields (EMF). One of the favourite systems are the membranes of nerve cells, e.g. in the central nervous system. Our aim is to clarify whether EMF exposure may induce athermal effects. In the experiments, direct electrophysiological *in vitro* measurements are conducted on neuronal networks exposed to EMF, i.e. possible changes in the action potential patterns produced by the networks are detected. The technique was developed as an alternative to the common patch-clamp approach.



Primary neuronal and glial cells were isolated from the frontal cortex of embryonic (E15 – E17) NRM1 mice. Chip [2] cultures were maintained at 37 °C in a 10 % CO₂ atmosphere for 30 days. The action potentials of the neurons were detected in real time by an integrated, electrically passive micro-electrode array (MEA). The neuronal cells grew directly on the MEA (Fig. 1). They reached their full electric activity after about 4 weeks. After this time, the networks were considered mature and suitable for experiments (Fig. 2). For EMF exposure the chips were introduced into a rectangular wave-guide (Fig. 3), that could be operated in the propagating or standing wave modes [1]. The drive signals were either CW (1.9 GHz - 2.2 GHz) or a generic mobile phone signal (UMTS-standard) of up to approx. 8 W (Fig. 4).

Method and Material

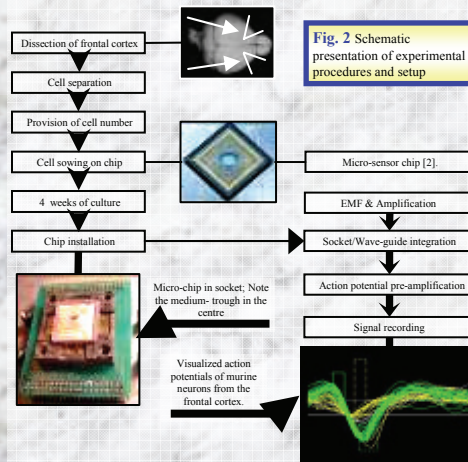


Fig. 3 Left: The wave-guide (1) is countersunk to pick up the micro-sensor chip in the socket (2). Right: View of the wave-guide with incoming signal line (3) and terminating resistor (4). The pre-amplifier is directly located under the chip socket (5). For actual experiments, the terminating resistor was connected via an appropriate extension cord and located outside the incubator to avoid an additional heat source.

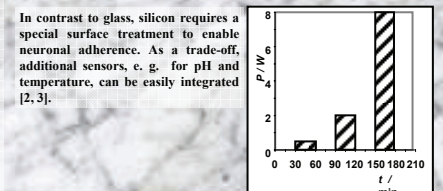


Fig. 4 EMF exposure pattern B

Wave-guide characteristics and EMF

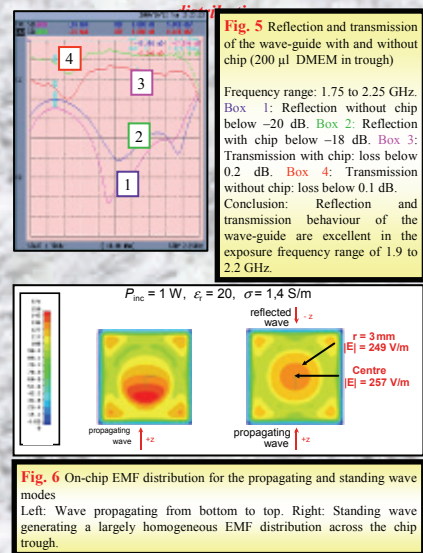


Fig. 6 On-chip EMF distribution for the propagating and standing wave modes. Left: Wave propagating from bottom to top. Right: Standing wave generating a largely homogeneous EMF distribution across the chip trough.

Results

Temperature courses

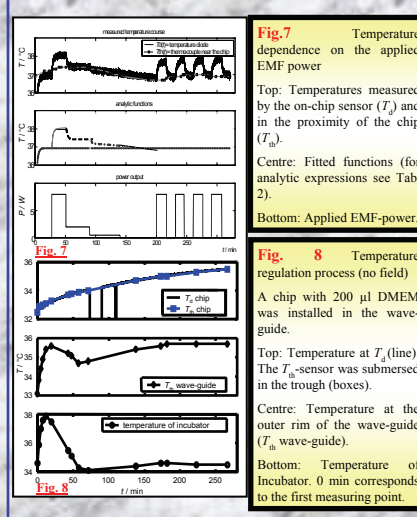


Fig. 7 Temperature dependence on the applied EMF power

Top: Temperatures measured by the on-chip sensor (T_1) and in the proximity of the chip (T_{in}). Centre: Fitted functions (for analytic expressions see Tab. 2). Bottom: Applied EMF-power.

Fig. 8 Temperature regulation process (no field)

A chip with 200 µl DMEM was installed in the wave-guide. Top: Temperature at T_1 (line). The T_1 -sensor was submersed in the trough (boxes). Centre: Temperature at the outer rim of the wave-guide (T_2 wave-guide). Bottom: Temperature of Incubator. 0 min corresponds to the first measuring point.

Signal recording & Signal type distinction

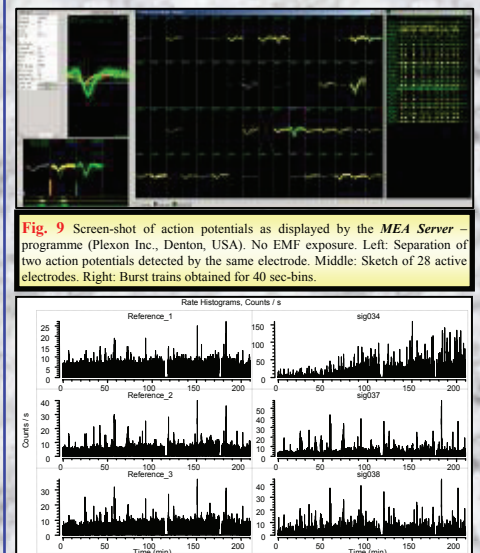


Fig. 9 Screen-shot of action potentials as displayed by the MEA Server - programme (Plexon Inc., Denton, USA). No EMF exposure. Left: Separation of two action potentials detected by the same electrode. Middle: Sketch of 28 active electrodes. Right: Burst trains obtained for 40 sec-bins.

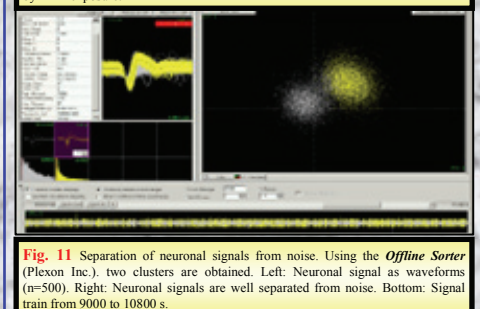


Fig. 10 Signals over time for exposure-pattern B as displayed by the NeuroExplorer software (Plexon Inc.). Left: Electrodes without neuronal cells exhibit only noisy signals. Right: Neuronal signals with high-noise peaks induced by EMF exposure.

Fig. 11 Separation of neuronal signals from noise. Using the Offline Sorter (Plexon Inc.), two clusters are obtained. Left: Neuronal signal as waveforms (n=500). Right: Neuronal signals are well separated from noise. Bottom: Signal train from 9000 to 10800 s.

Conclusion

Our preliminary results demonstrate the high potential of the approach. The wave-guide allows for a CW-EMF exposure in the frequency range from 1.9 GHz to 2.2 GHz in the propagating and standing wave modes and to a generic UMTS field in the propagating wave mode. Improving the input stage may reduce EMF-induced noise. Field distributions have been calculated for the the nourishing solution in the standing and propagating wave modes. Whereas the former generated a homogeneous field, the latter resulted in field gradient over the active chip area. Specific Absorption Rates can be derived.

Acknowledgments

This study has been supported by grant StSch 2002 0418A from the Bundesamt für Strahlenschutz (Federal Office for Radiation Protection). The authors would like to thank Dr. S. Homma for helpful discussions and the staff of the IZT (Institute for Cell Technology, Rostock-Warnemünde, Germany) for cooperation. The staff of the core facility "animal house" of the Dept. of Surgery at the University of Rostock's Medical Faculty is acknowledged for the reliable supply of mice. We are grateful to Prof. R. Meyer, Univ. of Bonn, for the kind provision of a wave-guide for preliminary tests. We would like to thank Dr. G. Friedrich from Forschungsgemeinschaft Funk for the donation of a generic UMTS-signal generator that was developed in the group of Prof. V. Hansen, Univ. of Wuppertal.

References

- [1] V. Hansen, J. Streckert, FGF, Edition Wissenschaft 14 (1998) 14-23.
- [2] W.H. Baumann, E. Schreiber, G. Krause, A. Podssun, S. Homma, R. Schrott, R. Ehret, I. Freund, M. Lehmann, Proceedings p-TAS 2 (2004) 554-556.
- [3] M. Lehmann, W. Baumann, M. Brischwein, H. J. Gahle, I. Freund, R. Ehret, S. Drechsler, H. Palzer, M. Kleintges, U. Sieben, B. Wolf, Biosensors & Bioelectronics 16 (2001) 195-203